



US006002424A

United States Patent [19]

Rapa et al.

[11] Patent Number: 6,002,424

[45] Date of Patent: Dec. 14, 1999

- [54] **DENTAL IMAGING SYSTEM WITH WHITE BALANCE COMPENSATION**
- [75] Inventors: **Frank G. Rapa**, Brooklyn; **Anthony A. Scott**, Bronx, both of N.Y.
- [73] Assignee: **Schick Technologies, Inc.**, Long Island City, N.Y.
- [21] Appl. No.: **08/873,805**
- [22] Filed: **Jun. 12, 1997**
- [51] **Int. Cl.⁶** **H04N 7/18**
- [52] **U.S. Cl.** **348/66; 348/68; 348/223**
- [58] **Field of Search** 348/65, 66, 68, 348/223, 224, 655; 600/160, 178, 180, 237, 238, 239, 240, 241

[56] References Cited

U.S. PATENT DOCUMENTS

1,704,397	3/1929	Meitzler	600/249
2,038,911	4/1936	Stutz et al.	240/2
2,788,390	4/1957	Sheldon	178/6.8
3,593,055	7/1971	Geusic	313/501
4,230,453	10/1980	Reimers	433/29
4,575,805	3/1986	Moermann et al.	364/474
4,858,001	8/1989	Milbank et al.	358/98
4,926,258	5/1990	Sasaki	348/70
4,994,910	2/1991	Williams	358/98

5,124,797	6/1992	Williams et al.	358/225
5,267,857	12/1993	Sickler	433/29
5,363,135	11/1994	Inglese	348/70
5,408,263	4/1995	Kikuchi	348/68
5,429,502	7/1995	Cooper et al.	433/29
5,487,661	1/1996	Peithman	433/29
5,512,036	4/1996	Tamburrino et al.	600/172
5,523,782	6/1996	Williams	348/66
5,527,261	6/1996	Monroe et al.	600/109
5,594,433	1/1997	Terlep	340/908
5,685,821	11/1997	Pike	600/118
5,691,772	11/1997	Suzuki	348/223
5,808,681	9/1998	Kitajima	348/223

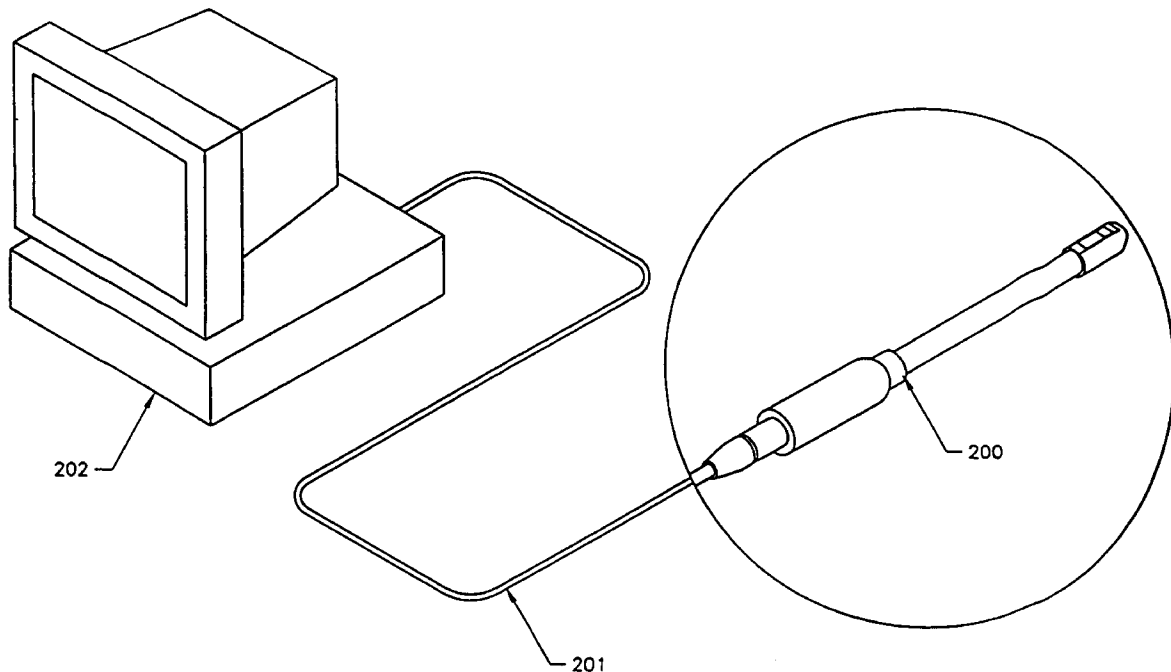
Primary Examiner—Bryan Tung

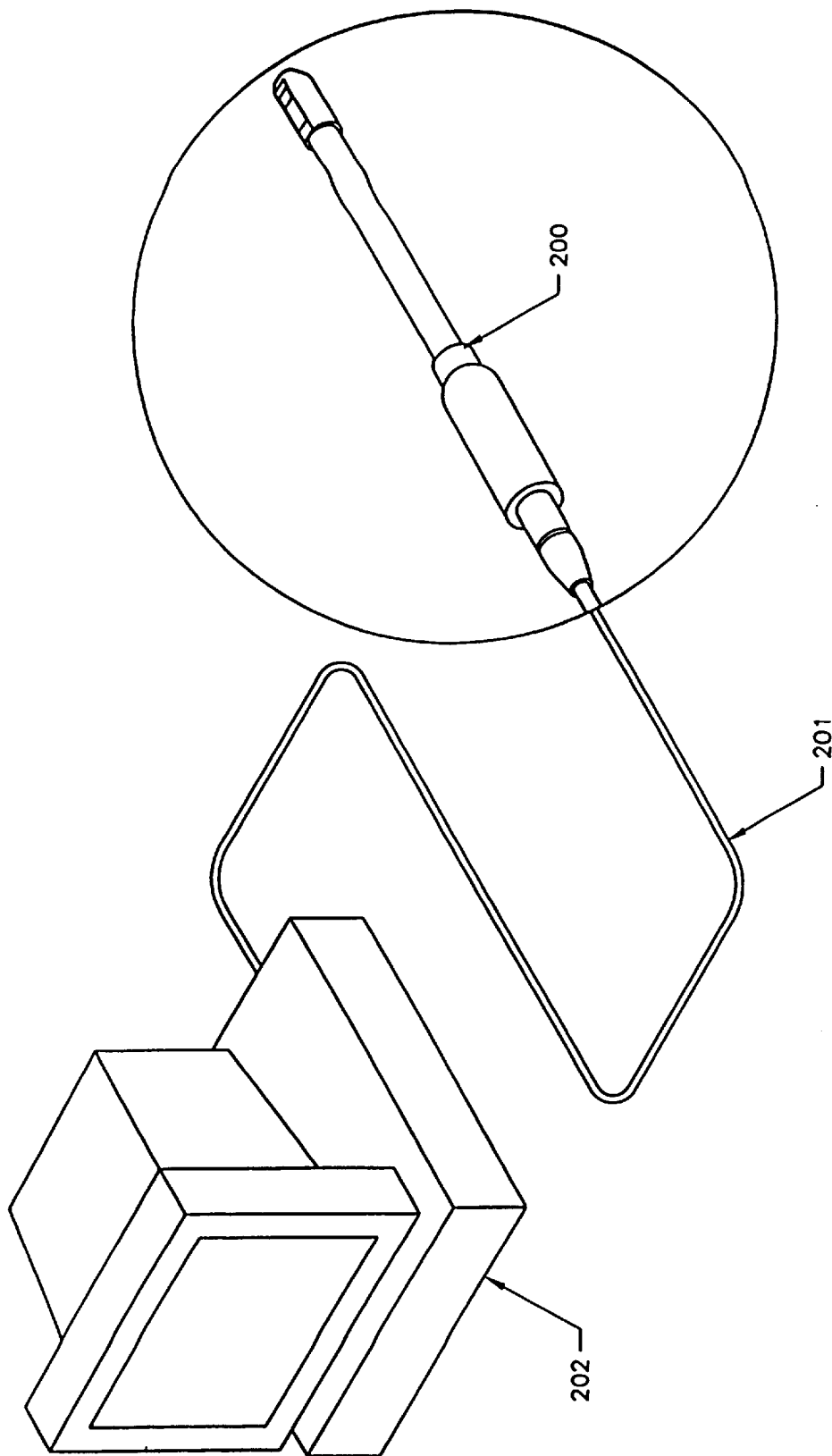
Attorney, Agent, or Firm—Fitzpatrick, Cella, Harper & Scinto

[57] ABSTRACT

An dental imaging apparatus and a corresponding method is disclosed. The imaging apparatus includes an image sensor, a lamp for providing illumination, and an image processor for processing the image in accordance with either a first stored white balance related to a characteristic of the lamp illumination or a second stored white balance. Preferably, the first stored white balance is used when the lamp is on, and the second stored white balance is used when the lamp is off.

20 Claims, 7 Drawing Sheets





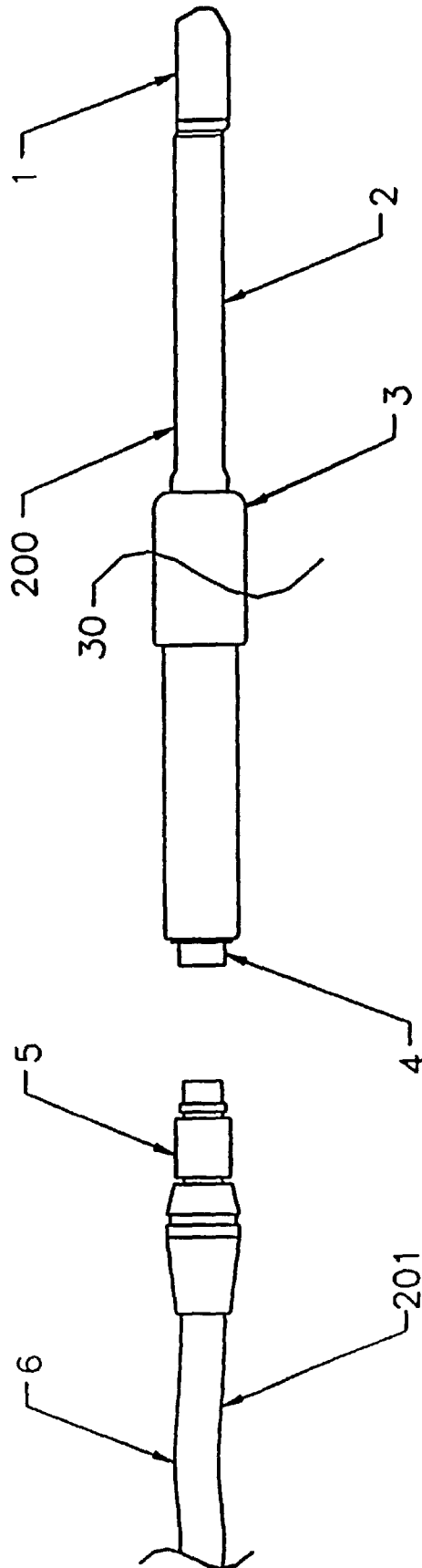


FIG 2

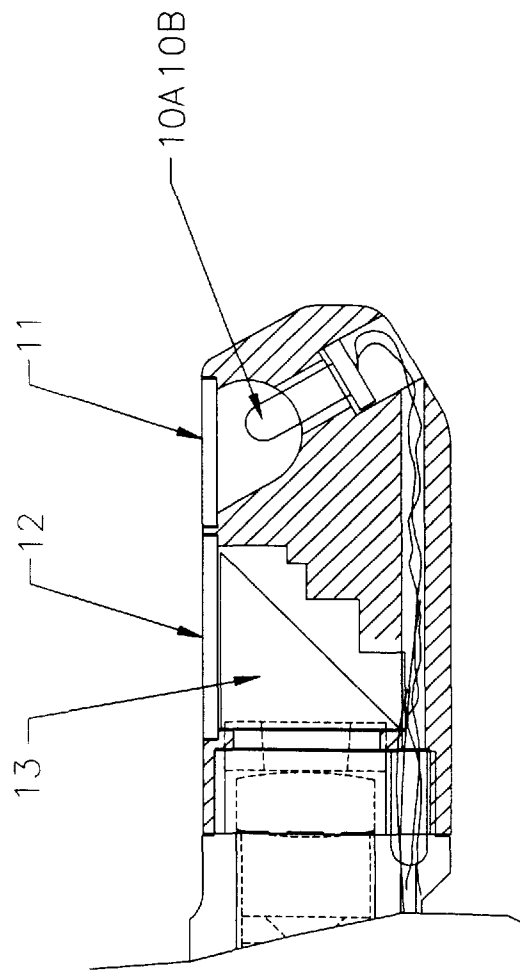


FIG 3A

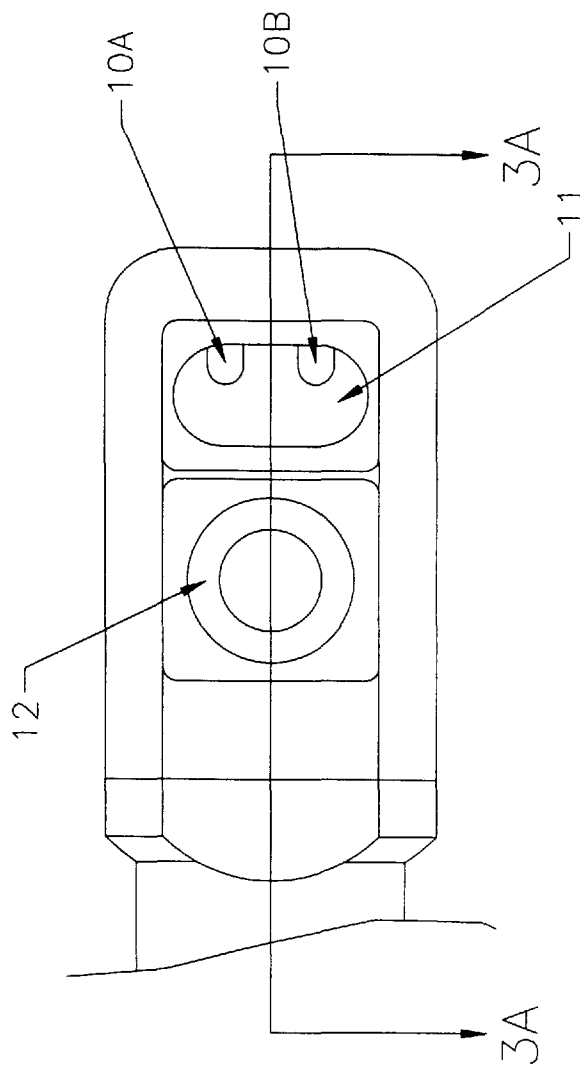
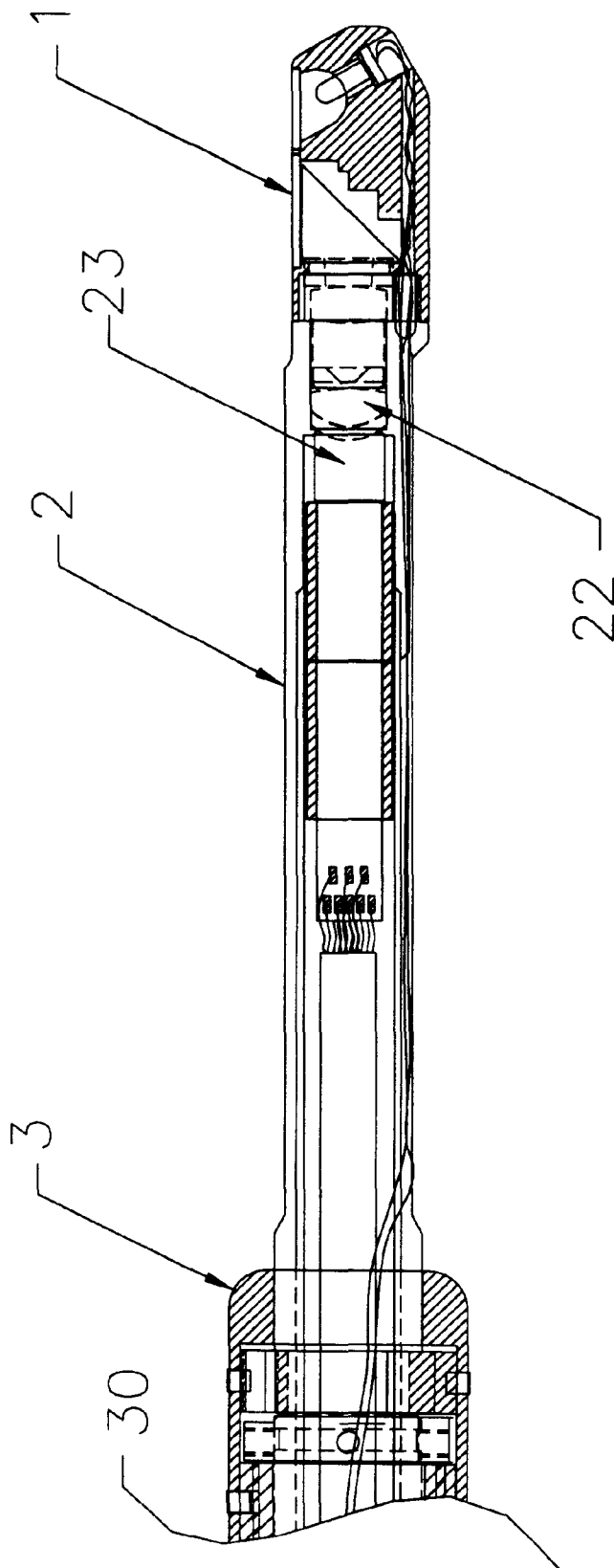


FIG 3B

FIG 4



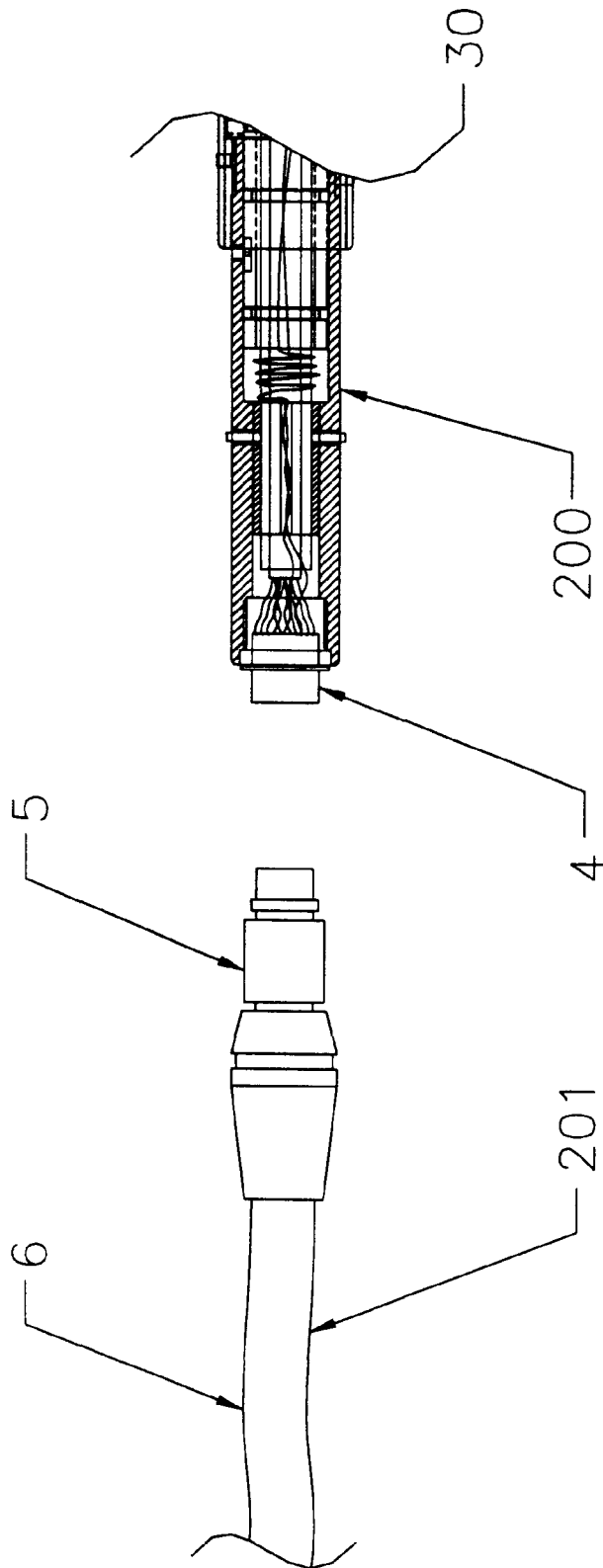
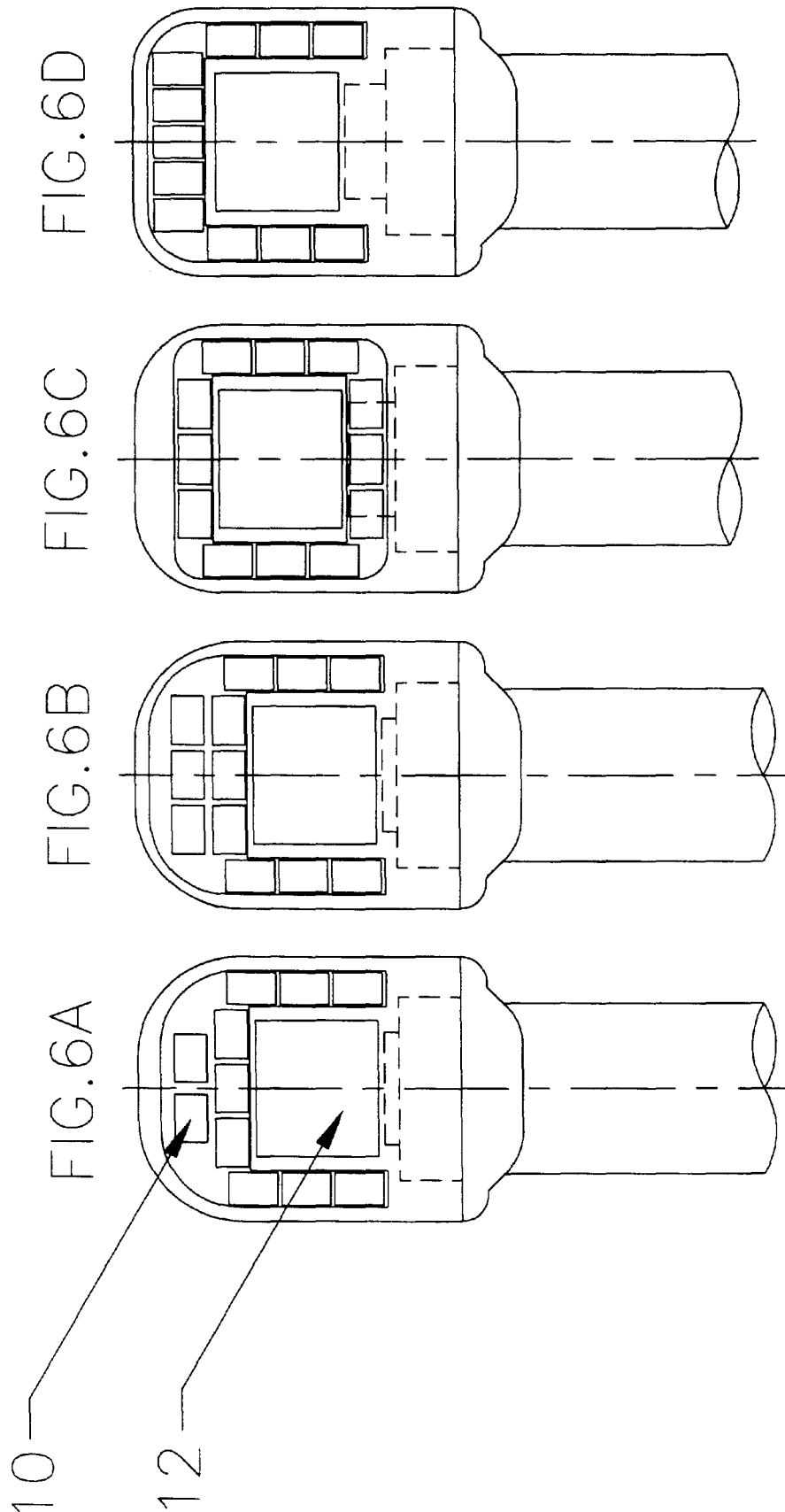


FIG 5



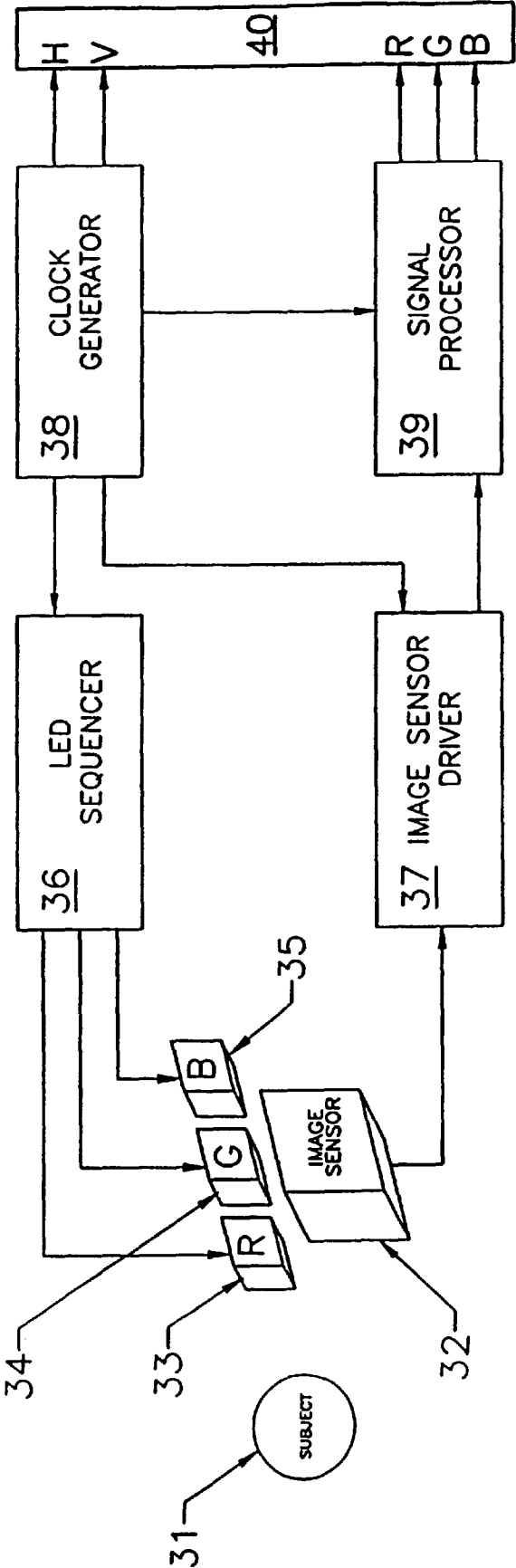


FIG 7

1

DENTAL IMAGING SYSTEM WITH WHITE BALANCE COMPENSATION

BACKGROUND OF THE INVENTION

This invention relates to the field of video imaging and, more specifically, to a video imaging apparatus for use in dental imaging.

Video imaging cameras have been used for obtaining images in dentistry for some time. One example of an existing system can be found in U.S. Pat. No. 5,523,782 (Williams), which describes a video dental camera that includes a light source, a CCD, and an adjustable focus lens system. Other examples of existing system can be found in U.S. Pat. No. 4,575,805 (Moermann et al.), and in U.S. Pat. No. 5,527,261 (Monroe et al.).

Until now, however, prior dental cameras did not rapidly and automatically compensate for the different white balances encountered (a) when the camera provides its own illumination and (b) when the camera is used with ambient illumination.

SUMMARY OF THE INVENTION

The present invention advantageously avoids the aforementioned drawback by compensating for the different white balances that may be encountered by a dental video camera.

According to one aspect of the invention, a dental imaging apparatus is provided. The apparatus includes a housing and an image sensor with an active surface. The image sensor is mounted in the housing so that the active surface receives light reflected from a dental subject. The apparatus also includes a lamp for illuminating the dental subject and an image processor for receiving image signals from an image sensor output and processing the image signals in accordance with either a first stored white balance related to a characteristic of the lamp illumination or a second stored white balance.

According to another aspect of the invention, a method of obtaining an image of a dental subject using an apparatus including a lamp and an image sensor is provided. The method includes the steps of receiving image signals from the image sensor and selecting a first or a second mode of operation. The image signals are processed in accordance with a first stored white balance related to a characteristic of the lamp when the first mode is selected, and in accordance with a second stored white balance when the second mode is selected.

According to another aspect of the invention, an apparatus for obtaining an image of a dental subject is provided. The apparatus includes a lamp, an image sensor, and means for receiving image signals from the image sensor. The apparatus also includes means for selecting a first or a second mode of operation and means for processing the image signals in accordance with a first stored white balance when the first mode is selected, and a second stored white balance when the second mode is selected. The first stored white balance is related to a characteristic of the lamp.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 depicts an embodiment of an electronic video dental camera and image processing system in accordance with the present invention.

FIG. 2 is an external side view of the camera showing the handpiece and the end of the connecting cord.

FIG. 3A is a cross-sectional view of a distal fragmented portion of the camera taken from section line 3A—3A in FIG. 3B.

2

FIG. 3B is a bottom view of the distal fragmented portion of the camera.

FIG. 4 is a cross-sectional view of the camera, showing detail in the median portion.

FIG. 5 is a view of the proximal portion of the handpiece and the distal portion of the connecting cord assembly.

FIGS. 6A–6D show alternate arrangements of lamps about the imaging window.

FIG. 7 is a block diagram of a strobed illumination system for the camera.

DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENTS

FIG. 1 shows a dental video camera system including a handpiece 200 and an image processing system 202. The handpiece 200 is connected to the image processing system 202 via a connecting cord 201.

FIG. 2 shows the handpiece 200 which has a distal end 1, a median section 2, a focusing ring 3, and a mini circular connector 4 at the proximal end of the handpiece. The connector 4 mates with a matching mini circular connector 5, which terminates the video cable 6. Signals originating from an image sensor (not shown) housed inside the handpiece 200 travel through the connector 4, the connector 5, and the video cable 6 on their way to the image processing system 202 (shown in FIG. 1).

FIGS. 3A and 3B show details of the distal end 1 of one embodiment of the handpiece, which includes an imaging window 12 and light sources 10a and 10b. The imaging window receives light reflected by the subject. The light sources 10a and 10b, which are located distal to the imaging window 12 and are covered by a protective glass shield 11, are aimed so that they will provide illumination for subjects located below the window. A prism 13 is located within the distal end of the handpiece 1, angled in relation to the imaging window 12 to direct the light arriving through the imaging window in the direction of the proximal end of the handpiece. Of course, instead of using an individual imaging window 12 and shield 11, as depicted in the figure, a single piece of material may be used as both the window and the shield. In this configuration, the material would have a window portion and a shield portion distal to the window portion.

A wide variety of lamps may be used. A low-power, long life lamp is preferable to save power and minimize service calls and system down time. One example of a suitable lamp is an incandescent light bulb, such as Gilway Technical Lamp #4115. Another example is a “white LED”. This white LED could comprise, for example, a short-wavelength LED combined together with a phosphorescent coating, such as Nichia America #NSCW-100. The “white LED” could also comprise, for example, a set of three single color LEDs (e.g., red, green, and blue), mounted in a single package, such as Nichia America #NSCM-310. While two lamps are depicted in the figure, any number of lamps may be used. In addition to generating light, the lamps also generate some heat. This is advantageous in dental applications, because it helps clear away condensation that could form from a patient’s breathing on a cold instrument.

By locating the lamps in the distal end of the handpiece, distal to the imaging window, and angling the lamps so as to provide direct illumination of the object being imaged, the diameter of the housing can be minimized. This allows the present invention to be contained within a slimmer housing, as compared to prior art cameras which have light sources

positioned above the imaging window, such as the one described in U.S. Pat. No. 4,575,805 (Moermann et al.). A slimmer device is advantageous for dental use.

Alternative light source arrangements may also be used. For example, FIGS. 6A, 6B, and 6D show a number of light sources **10** arranged on three sides of the imaging window **12**. FIG. 6C shows a number of light sources arranged on four sides of the imaging window. Numerous other light source arrangements can be readily envisioned.

Aiming of the light sources depends on both the arrangement of the light sources around the window and the type of light source used. For example, when incandescent lamps are used in the configuration shown in FIG. 3B, the lamps should be angled as shown in the figure so that the light is directed back towards the proximal end. When LEDs are used in any of the configurations depicted in FIGS. 6A–6D, the LEDs can be aimed perpendicular to the surface of the instrument, because the light is sufficiently diffused to illuminate the subject.

FIG. 4 shows details of the median section **2** of the handpiece, which houses the lens system **22**, the image sensor **23**, and the focusing mechanism **3**. The lens system **22** is preferably a fixed-focus lens system. The image sensor **23** is preferably either a CCD (charge coupled device) or an APS (active pixel sensor array).

The lens system **22** is located in the distal portion of the median section **2**, proximal to the distal end of the handpiece **1**. The movable image sensor **23** is located proximal to the fixed lens system **22**. The lens system **22** transmits the light arriving from the distal end of the handpiece **1** to the active surface of the image sensor **23**. The lens system **22** may be replaced by another type of light direction means including, for example, a mirror, a prism, and an optical fiber.

The movable image sensor **23** is controlled by a plunger system which is attached to the focusing ring **3**. Preferably, the focusing ring **3** can be manually rotated into any of a plurality of detented positions that correspond to a plurality of image sensor positions.

One preferred embodiment uses four detented positions. When the focusing ring **3** is rotated into each of the four various positions, the image sensor, which is mechanically coupled to the plunger system, is moved nearer to or farther from the fixed lens system **22** along a proximal-to-distal axis, depending on the degree of rotation. Each of these positions has an associated focal setting and depth of field. Most preferably, the approximate focal range settings are: (1) 1 to 6 mm; (2) 5–15 mm; (3) 12–25 mm; and (4) 180 mm– ∞ . This selection of focal range settings is optimized for dental imaging by minimizing the required amount of manipulation while maximizing image quality and ease of use. For a system using a 3.65 mm×2.74 mm rectangular CCD image sensor and a lens with a focal length of 4.50 mm, the total range of movement of the image sensor needed to obtain these focal settings is approximately 2 mm. If the amount of light supplied to the subject is increased, the depth of field can be extended by reducing the aperture of the lens. This would allow a reduction in the number of focus ranges.

FIG. 5 shows a sectional view of the proximal end of the handpiece **200**, as well as the distal end of the connecting cord assembly **201**. The mini circular connector **4** at the proximal end of the handpiece **200** mates with the connector **5** on the connecting cord assembly **201**. Preferably, the connectors can be mated and released quickly. A suitable connector pair for this purpose includes, for example, parts Nos. HR25-9P-16 and HR25-9R-16 made by Hirose Elec-

tric. The connecting cord assembly **201** includes a video cable **6** which is preferably flexible and lightweight. When the connector **4** is mated with the connector **5**, the connecting cord assembly transmits the video image acquired by the image sensor in the handpiece to the image processing system (shown in FIG. 1). Some preprocessing (including, e.g., preamplification) may be performed by known means in the handpiece **200** before the image signals are sent to the image processing system.

Returning to FIG. 1, the image processing system **202** may be implemented in hardware, software or a combination of both. Two image processing settings may be selected: intraoral and extraoral. These settings correct for the quality and amount of light available and allow for realistic images to be acquired in both intraoral and extraoral locations, because ambient light is qualitatively different from lamp light. This feature is implemented by storing two different white balances in the image processing system (one for the extraoral setting and one for the intraoral setting) and processing the image using the appropriate stored white balance. The white balance processing adjusts the levels of the red, green, and blue components of the image to create an image in which white objects are perceived as being white.

A preferred approach of implementing the white balance processing uses the Panasonic GP-KS 162 CB camera control unit (CCU) together with a Panasonic GP-KS 462HM CCD. The CCU includes circuitry to interface with the CCD, white balance processing, and circuitry to generate an NTSC video signal. The CCU can store two white balances corresponding to two different types of light. For example, the white balance settings for the ambient light coming from a dentist's overhead light and from the camera's light source can be stored. When the dentist uses the camera, the appropriate white balance setting can be selected instantaneously without recalibrating the white balance for each exposure.

The preferred CCU can compensate for white balances ranging from 2,200–10,000 ° K. of color temperature. Incandescent lamps and both types and white LEDs are available within that temperature range. For those parts that have a wide range of color temperature, samples with the appropriate color temperature should be selected.

In the case of intraoral imaging, very little ambient light is available. When the camera is switched to the intraoral setting, the light source located in the head of the camera can be automatically switched on. In this mode, the image is processed using a stored white balance corresponding to the quality of the lamps which provide illumination (e.g., the incandescent bulbs or LEDs described above). In the case of extraoral imaging, ambient light is available. When the camera is switched to the extraoral setting, the light source can be automatically turned off. Due to the presence of ambient light, a different stored white balance is used to process the image.

The embodiments described above involve illuminating the subject with white light and detecting the light using a sensor that is sensitive to white light. An alternative embodiment uses a monochromatic sensor and strobes of different colored monochromatic light to attain the same effect as white illumination.

FIG. 7 depicts an embodiment that uses this strobed configuration. In this embodiment, instead of illuminating the subject with white light, the subject is strobed with each of the components of white light (red, green, and blue) sequentially. During each strobe period, the output from the

image sensor is captured. The image sensor outputs from the three strobe periods are then combined by a signal processor to form a standard RGB video signal.

The clock generator 38 provides timing signals to synchronize the circuit. The LED sequencer 36 receives a clock signal from the clock generator 38, and turns on each of the LEDs 33–35 in turn, in three phrases. During the first phase, the LED sequencer 36 turns on the red LED 33. During the second phase, the LED sequencer 36 turns on the green LED 34. During the third phase, the LED sequencer 36 turns on the blue LED 35. This sequence of phases repeats continuously.

The clock generator 38 also sends signals to the image sensor driver 37. The image sensor 32 receives light that originated from one of the LEDs 33–35, bounced off a subject 31, and onto the image sensor 32. The output of the image sensor is received by the image sensor driver 37. When the red LED 33 is illuminated, the image sensor will capture an image of the subject 31 illuminated by red light. When the green LED 34 is illuminated, the image sensor will capture an image of the subject illuminated by green light. Similarly, when the blue LED 35 is illuminated, the image sensor will capture an image of the subject illuminated by blue light.

The signal processor 39 receives these three images from the image sensor driver 37, together with synchronizing signals from the clock generator 38. The signal processor combines three image signals into ordinary RGB signals which are provided to a video signal interface 40. The clock generator 38 provides horizontal and vertical synchronization signals to the video signal interface 40, which outputs a video signal in a standard format such as NTSC, PAL, etc.

It is also possible to implement an equivalent system by illuminating the subject with more than one color at a time. For example, red light may be used during the first phase, and red and blue light may be used during the second phase. Then, the blue component may be computed by subtraction. Of course, other combinations of colors may be used as well.

By using this system, a monochromatic image sensor may be used in place of a full color image sensor. This is advantageous because monochromatic image sensors are significantly less expensive. In this configuration, to achieve a standard video frame rate of 30 frames per second, the frame rate at the image sensor must be tripled (i.e., to 90 frames per second). As a result, one red, one green and one blue image is captured by the image sensor in each $\frac{1}{30}$ second interval. These images are stored in the signal processor 39 and output at the standard frame rate.

Preferably, the signal processor 39 includes white balance circuitry that adjusts the proportions of the red, green, and blue images to produce a color-corrected image. Alternatively, the LED sequencer 36 can vary the brightness and/or duration of the red, blue, and green illumination to achieve color corrected images.

The combination of features described above allows the camera to be lighter, more portable, consume less power, and to produce a more authentic image than previous cameras.

While the present invention has been described above in terms of specific embodiments, it is to be understood that the invention is not limited to the disclosed embodiments. On the contrary, the present invention is intended to cover various modifications and equivalent structures included within the spirit and scope of the appended claims.

We claim:

1. A dental imaging apparatus comprising:

a housing;

an image sensor having an active surface, said image sensor being mounted in said housing so that the active surface receives light reflected from a dental subject;

a lamp, mounted in said housing, for illuminating the dental subject when said lamp is on;

a switch that selects between an intraoral mode in which said lamp is on and an extraoral mode in which said lamp is off; and

an image processor that receives image signals from said image sensor and processes the image signals in accordance with either a first stored white balance when said switch is set to select the intraoral mode or a second stored white balance when said switch is set to select the extraoral mode.

2. The dental imaging apparatus according to claim 1, wherein the first stored white balance is optimized for the light provided by said lamp.

3. The dental imaging apparatus according to claim 1, wherein the second stored white balance is optimized for ambient light.

4. The dental camera imaging apparatus according to claim 1, wherein said lamp comprises an incandescent light bulb.

5. The dental imaging apparatus according to claim 1, wherein said lamp comprises a plurality of different colored LEDs.

6. The dental imaging apparatus according to claim 1, wherein said lamp comprises an LED and a phosphorescent coating.

7. The dental imaging apparatus according to claim 1, wherein said image sensor comprises at least one of a CCD and an APS.

8. The dental imaging apparatus according to claim 1, further comprising a quick release circular connector mounted on said housing, said connector being electrically connected to the output of said image sensor, said connector being capable of mating with a compatible connector for sending signals to said image processor.

9. A method of obtaining an image of a dental subject using an apparatus including a lamp and an image sensor, the method comprising the steps of:

receiving image signals from the image sensor;

selecting between an intraoral mode in which said lamp is on and an extraoral mode in which said lamp is off;

processing the image signals in accordance with a first stored white balance when the intraoral mode is selected; and

processing the image signals in accordance with a second stored white balance when the extraoral mode is selected.

10. The method according to claim 9, further comprising the step of causing the lamp to illuminate the dental subject when the first mode is selected.

11. The method according to claim 10, wherein the first stored white balance is optimized for the light provided by the lamp.

12. The method according to claim 10, wherein the second stored white balance is optimized for ambient light.

13. An apparatus for obtaining an image of a dental subject comprising:

a lamp;

an image sensor;

means for receiving image signals from said image sensor;

7

means for selecting between an intraoral mode in which said lamp is on and an extraoral mode in which said lamp is off; and

means for processing the image signals in accordance with a first stored white balance when the intraoral mode is selected, and processing the image signals in accordance with a second stored white balance when the extraoral mode is selected.

14. The dental imaging apparatus according to claim **13**, wherein the first stored white balance is optimized for the light provided by said lamp.

15. The dental imaging apparatus according to claim **13**, wherein the second stored white balance is optimized for ambient light.

16. The dental imaging apparatus according to claim **13**, wherein said lamp comprises an incandescent light bulb.

8

17. The dental imaging apparatus according to claim **13**, wherein said lamp comprises a plurality of different colored LEDs.

18. The dental imaging apparatus according to claim **13**, wherein said lamp comprises an LED and a phosphorescent coating.

19. The dental imaging apparatus according to claim **13**, wherein said image sensor comprises at least one of a CCD and an APS.

20. The dental imaging apparatus according to claim **13**, further comprising a quick release circular connector mounted on said housing, said connector being electrically connected to the output of said image sensor, said connector being capable of mating with a compatible connector for sending signals to said image processor.

* * * * *